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Which Factors have an Impact on the Retention of Cemented Crowns on Implant Abutments? A Literature Review

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Abstract

Background: The review presents the scientific state of the art in the field of cementation of crowns on implants. Because semipermanent cements have been specially developed for the cementation of crowns on implants, the question arises whether this cement group offers an advantage compared to other available and widely used cements in everyday clinical practice. Various factors play a role on the retentive strength of superstructures on implants and should therefore be taken into account in this review.

Materials and methods: A thorough search of the literature, mainly PubMed as well as a manual search, was conducted between 2005 and 2020 to screen relevant articles for data regarding retention forces of different cements used on single crowns and implants by three independent investigators. 37 studies were included in this review because they met the inclusion criteria (prospective and an *in vitro* study design about implant-supported single crowns; English language; all-ceramic or metal-ceramic superstructures on titanium or zirconia implants) and did not relate to the exclusion criteria (fixed dental prostheses, articles describing other studies; reviews and clinical studies; screw-retained single crowns; neglecting the focus on the retention force after cementation).

Results: In recent years, a high number of various cements for use on implants have been scientifically investigated. A wide range of retention values have been published for each cement type. Furthermore, various influencing factors exist regarding retention of semipermanent cements. Significant correlations have been demonstrated between retention force and cement type, crown pretreatment, taper, abutment surface, internal surface cleaning, cement gap, and the presence of grooves on the abutment (Pearson's bivariate correlation; P<0.01 and P<0.05). Artificial ageing, such as a chewing simulation, have been neglected so far in the majority of studies. Thermocycling mostly reduced retentive strength.

Conclusion: This review revealed that there are several influencing factors on the retention of crowns which were temporary cemented on implants abutments. It could be shown that there are significant correlations between retentive strength and different parameters. Due to the inconsistent data situation caused by noncomparable study methodologies, the question of the whether semipermanent cements is superior to the conventional definitive or conventional provisional cements available cannot yet be answered.

Keywords: Implantology; Cementation; Semipermanent; Single crowns; Retention

Abbreviations: N: Newton; CAD/CAM: Computer Aided-Design/ Computer Aided-Manufacturing

Background

Implant-supported crowns can be retained by screws or cement. The advantages of screw fixation primarily affect the peri-implant tissue [1]. A further advantage is the option of accessing the screw channel to loosen or reattach the implant-supported restoration easily [2-5].

Technical complications, including loosening or fracture of the abutment screw, occurred significantly more often with screwretained single crowns than they did with cement-retained single crowns [6]. Although cemented crowns on implants have a lower rate of technical complications compared to screw-retained crowns, they are often only temporarily cemented.

The advantage of cementation is that it is independent of the axial alignment of the implants. Esthetic limitations caused by the visible access are eliminated with cementation [7]. Finally yet importantly, the clinical procedure of cementation is firmly anchored in the everyday practice of dentists. The procedure can be carried out routinely [3,8].

With regard to cementation of the superstructure on implants, a distinction is made between temporary and permanent cements. The bond strength values differ significantly between the bond to



implant abutments and natural teeth. In particular, zinc phosphate, zinc polycarboxylate and glass ionomer cements showed a wide range between retention values [9-12]. Nevertheless, these cements, including self-adhesive resin cements, are used for permanent cementation of single-tooth crowns on implants [13]. They also serve as comparative values in scientific studies regarding retention values [4,10,13,14]. However, provisional cements, such as zinc oxide or eugenol cements, have been recommended for cementation in other studies because of the possibility of retrievability [4,13,15,16] and to allow non-destructive removal of the crown in case of screw loosening. Different studies have described and recommended this treatment option [17-19]. A disadvantage is that temporary cements have poor physical properties. These include high solubility and low tensile strength [4,13,16].

Previous studies have recommended that definitive cements should be used for the cementation of single-tooth restorations and provisional cements for the cementation of multi-unit restorations [9,20,21], as larger restorations may be more likely to require retrievability. Definitive resin cements are the cement of choice for definitive cementation of single-tooth restorations [9,22,23]. In general, there is a disagreement as to whether temporary or definitive cements should be used for superstructures on implants [17,18,20,24].

Furthermore the industry offers special cements (ie, semipermanent cements) for the use on implants. They have become popular in recent years because they combine the advantages of removability and increased retentive strength [25].

Because implant abutments are not susceptible to caries, it appears that in addition to the classical properties of cements, such as high biocompatibility, low solubility, easy manipulation, and a sufficiently long working time [26,27], the primary focus is on the required retention. It should be high enough to prevent spontaneous loosening of the crown. Furthermore, semipermanent cements should have the property whereby the restoration can be detached from the tooth or abutment without destruction.

Currently, no official classification exists for provisional, semipermanent, and definitive cements regarding retention values.

It is known that there are various factors influencing successful cementation and adequate retention. A cement gap of 20-40 μ m is considered ideal [13,28-31]. This should allow the outflow of excess cement and consequently guarantee adequate seating forces of the restoration [13]. Other influencing factors such as the abutment surface size, the taper, the geometry of the abutment or the pretreatment of the internal surface of the crown have already been investigated in previous studies and identified as factors influencing retention [18,32-34].

To test the hypothesis that different factors have an influence on retention of temporary cementation of crowns on implant abutments and semipermanent cements do not have relevant advantages compared to conventional definitive cements and conventional temporary cements, a thorough search of the literature was conducted to summarize the data gained so far about cementation on implants.

Materials and Methods

For this review, a thorough search of the literature was done. The primary database used was PubMed. Additionally, the search was supported by a manual search to check references of relevant studies to find more useful publications. Inclusion, exclusion, and eligibility criteria were calculated to develop a specific search strategy (Tables 1-5). The time range of 2005 to 2020 was chosen for selecting the Table 1: Inclusion criteria.

Study Design	Prospective; in vitro
Language	English
Prosthetic type	Implant-supported single crowns
Material (superstructure)	All-ceramic, metal-ceramic
Material (implant + abutment)	Titanium, zirconia
Year of publication	2005-2020

Table 2: Eligibility criteria.

Eligibility criteria
Any kind of root-form implant with a single crown as the superstructure
cemented with different types of cements (definitive, semipermanent,
and temporary) to compare retention values after pull-off tests. There
were no restrictions regarding the type of implant.
L

Table 3: Exclusion criteria.

Exclusion criteria
Fixed dental prostheses
Articles describing other studies
Reviews and clinical studies
Screw-retained single crowns
Focus not on retention force after cementation

 Table 4: Overview of the average retention forces for different kinds of cementation.

Cementation	Retention (N) (after water storage)	References	Duration		
		Botega 2004 [35]			
Tomoroway	7 100	Lehmann 1976 [36]	Weeks		
Temporary	7-100	Mehl 2010 [3]	1		
		Breeding 1992 [17]			
		Covey 2000 [37]			
Cominormonont	50.000	Di Felice 2007 [38]	Medium to		
Semipermanent	50-200	Dudley 2008 [23]	iong term		
		Kaar 2006 [39]			
	Polycarboxylate				
Definitive	cements: 307 ± 96	Mobl 2012 [2]	Long term		
Demittive	Resin-based	Well 2013 [3]	Long term		
	cements: 480 ± 48				

 Table 5: Percentage changes of the decementation load related to abutment height for different cement classes.

Comont	Changes of the decementation load (%)							
Cement	4.0 mm	5.5 mm						
Zinc oxide, eugenol-free	-45	-90						
Zinc phosphate	-4	+92						
Glass ionomer	+23	+33						
Resin based, self-adhesive	+35	+16						
Methacrylate based	-80%	-68%						

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studies (Table 1). The following article types were chosen: journal article, case report, classical article, clinical study, and clinical trial protocol. Regarding the search strategy, a combination of medical subject heading terms and free text words was applied. Various keywords were used to find relevant articles appropriate for answering the hypothesis ("dental AND implant AND crown AND cementation AND retention" and other combinations).

The retention forces found in the studies and the factors influencing them were summarized in table 6. The correlation between relevant factors and the retention force was determined using Pearson's correlation test (IBM SPSS Statistics for Windows, version 27.0. Armonk, NY, USA, 2020) (Table 7).

Results

Study selection

The results of the literature search were 329 hits for the Medline search for the period between 01/01/2005 and 12/01/2020 (last search date: 12/22/2020). For these initially identified papers, 60 articles were excluded because they did not meet the inclusion criteria (Tables 1,3). Two hundred and sixty-nine were screened regarding the titles and abstracts. A further 212 articles were excluded because of the mentioned inclusion and exclusion criteria (Tables 1,3). From checking references, 2 additional articles were found that met the criteria. As a result, 57 articles were evaluated by full-text analysis. In the end, 37 articles were used as data for the analysis in this review (Figure 1, Table 7).

Comparison of retentive strength for different types of cement

The literature search revealed the following retention values for temporary, semipermanent and definitive cements: For temporary cements, it is important to know the range in which the retention force may be in order to be able to remove the restoration undamaged. At the same time, the retention must be appropriately high to prevent loosening of the crown in everyday use [15,17]. For temporary cementation retention values between 7-100 Newton (N) are considered appropriate (Table 4) [3,35,36]. The minimum value of 7 N results from the retention values for partial dentures that generate sufficient denture retention in the range of 3.5-7 N [35,36]. The maximum value of 100 N is based on investigations by Mehl C, et al., [3]. Therefore, the number of strokes needed to loosen a cemented implant crown from an abutment was measured [3]. A static force of about 21 ± 5.6 N per blow and 10 attempts on average were needed for a dentist to loosen the crown. The upper limit was set to 100 N, which corresponds to approximately 5 blows [3].

For semipermanent cementation, retention values between 50 and 200 N were measured (Table 4) [17,23,37-39]. In this area, sufficient retention of the crown on the abutment should be ensured. Alternatively, damage-free removal of the crown should be possible if required. Therefore, resin cements with low solubility have been developed in recent years. However, only limited data are available regarding retention values of these newly developed resin cements
 Table 6: Significant correlations between retention force and various parameters as well as the P value.

Parameter	Retention in Newton (N)	P value
Cement	-0.205**	0.000
Pretreatment internal crown surface (sandblasting)	0.158**	0.000
Taper	-0.211**	0.000
Cleaning internal crown surface (alcohol)	-0.153**	0.001
Abutment surface size	-0.118*	0.034
Cement gap	-0.232*	0.031
Grooves on abutment	0.139**	0.002

*P< 0.05, **P< 0.01

created especially for semipermanent cementation of superstructures on implant abutments [13,15,40].

As representatives of the definitive cements, glass ionomer cements, polycarboxylate cements, and resin-based cements were used and tested in most studies [4]. After 3 days of water storage and a pull-off test, the following retention values were obtained for the cements mentioned for a 50 μ m cement gap: glass ionomer cements 144 \pm 53 N; polycarboxylate cements 307 \pm 96 N; and resin-based cements 480 \pm 48 N (Table 4) [4].

Parameters influencing retention forces

Cement film thickness: The included studies that examined the cement film thickness showed that for the glass ionomer cement, retention was reduced by 28% between the 50 μ m cement gap and the 80 μ m cement gap, respectively, and the 110 μ m cement gap. The same did the polycarboxylate cement (-69%). The resin-based cement showed homogeneous values for all 3 cements' gap thicknesses [3].

Furthermore great differences existed between the retentive strength before and after thermocycling for the tested temporary cements [41]. Retention values were significantly lower after thermocycling and it also influenced the cement film thickness significantly [41].

Artificial ageing

Artificial ageing (thermocycling) showed in the majority of the studies that retention decreased afterwards [9,14,24,40-56]. Studies that carried out measurements before and after thermocycling published reduced retentive strengths of about 68% for noneugenol acrylic/urethane resin-based temporary cement, 88% for zinc oxide noneugenol cement, and 94% to 98% for 3 different dual-polymerizing semipermanent resin cements [43].

Effects of compressive cyclic loading on the retention of implant-supported crowns are only available to a limited extent [40,50,51,53,57,58]. Compressive cyclic loading leads to a reduced retention of the superstructure of about 50% for glass ionomer cement, 53% for compomer cement, and 59% for resin urethane-based cements [58].

Sandblasting

The majority of included studies performed sandblasting as a pretreatment of the internal surface of the crowns. The influence of thermocycling and sandblasting on retention was found to affect both components more or less significantly, depending on the cement type [14]. Zinc oxide cements showed the highest retentive strength. Sandblasting was effective for improving the durability. For the other tested cements, the effect of sandblasting was negligible. The retentive strength of zinc oxide cements decreased significantly after thermocycling, even with sandblasting. Consequently, zinc oxide cements were not recommended for the cementation of single crowns on implants [14].

Different geometry of the abutments

With regard to 2 different abutment heights (4.0 and 5.5 mm), it was shown that a higher abutment exhibited higher retention values for all tested cements except zinc phosphate cement after water storage (Table 5).

Bivariate correlation analysis

Pearson's correlation results revealed significant correlations between retention force and various parameters (Tables 6,7). The correlations were significant at the level of p<0.01 and p<0.05, 2-sided, respectively.

Discussion

Regarding the hypothesis that different factors have an influence on retention of temporary cementation of crowns on implant abutments, this literature review showed, that significant correlations between some factors could be proven. As a consequence, when interpreting the retention, it is important to note that it depends not only on the cement properties but also on factors such as the abutment geometry (angle, length, taper and height) and the surface size of the abutment [4]. A significant correlation between retention force and the taper could be shown. The usual taper of abutments is 6° [4]. Smaller tapers increase the retention, but make cement flow more difficult and can lead to an increase of the occlusion. Larger conicities lead to increased pull-off forces acting on the cement. Retention is therefore closely related to the preparation and decreases with increasing taper [2].

Furthermore the abutment surface size and the abutment geometry (grooves) showed significant correlations regarding retention force. In general, factors such as the abutment height, the diameter, and the surface area have a positive effect on the retention of crowns on abutments [54,59-64]. Height and surface are closely related [7]. The higher the surface and the height of the abutment are, the higher the retention is [3,18]. The effect might lose importance when adhesive resin-based cements were used [59]. Axial wall modifications also showed positive effects on retention [65]. Other surface configurations did not always show higher retention values [24]. Additional grooves also increased retention [44]. However, Carnaggio TV, et al., [59] used 3 abutments of different surface sizes (42, 60, and 82 mm²). The results were heterogeneous because the height of the different abutments was the same. Only the circumference was increased. Therefore, there is no linear relationship and a corresponding increase in the pull-off forces between the smallest and the largest abutment surface. For the 2 selfadhesive resin cements, retention values increased by 24% and 73% from the 42 to 82 mm² abutment surface. However the resin-modified glass ionomer cement showed the opposite development (-42%). Zinc oxide, noneugenol cements only exhibited increased retention values of about 37% between the smallest and the largest abutment surface sizes. The acrylic-urethane provisional cement showed the highest retentive strength at the middle-abutment surface size.

The cement gap also showed a significant correlation regarding retention. According to Mehl C, et al., [3], the cement film thickness has an influence on retention of the superstructure even if crowns are designed with the help of Computer aided-design/Computer

aided-manufacturing technology (CAD/CAM) to obtain identical restorations and thus to obtain a homogeneous cement gap [3]. In addition, each specimen, consisting of a crown and abutment, should only be used once to eliminate possible sources of error [59]. Cement residues could damage the abutment surfaces during cleaning. A second cementation would falsify the results [59].

A precise statement with regard to the hypothesis regarding semipermanent cements cannot be made at this time. It can neither be confirmed nor completely rejected. The data situation is heterogeneous. A clear definition of the term semipermanent cementation does not yet exist. Based on this review, a precise definition cannot be established. The biggest problem here is the durability of the crown and various influencing factors. An unambiguous classification into definitive, semipermanent, and temporary cements is hardly possible. In general, retention values of the individual cements differed greatly in various studies. Therefore, some studies published guidelines for clinicians because no cement served for all demands [13,66]. Furthermore, the retention values were very different in the individual material classes and therefore not comparable [13]. In detail, it was found that glass ionomer cements might be suitable for semipermanent cementation [4,41,45,46,60] because retention forces should lie between 50-200 N for semipermanent cementation [17,23,37-39]. Glass ionomer cement develops its full retention over time. In most studies, pull-off tests were immediately performed 24 hours from when the cementation took place. At this time, full retention of the glass ionomer cements had probably not yet been achieved [59]. The use of temporary cements, particularly eugenol-free zinc oxide phosphate cements, led to reduced retention values, especially after thermocycling [43,54,59,67]. Consequently, they are not suitable for semipermanent cementation. If retrievability is required after a short time, they might offer a solution to ease removal of the crown [4,59,68]. Self-adhesive resin cements, zinc oxide cements, and polycarboxylate cements showed mostly higher retentive strengths regardless of the crown material compared to temporary cements [4,24,69,70]. However, retrievability is not possible without destruction of the superstructure [23,71-73].

The correlation analysis showed that certain parameters could have a relevant influence on the retention force of cements. These include cement type, pretreatment and cleaning of the internal crown surface, taper, abutment surface size, cement gap, and grooves on the abutment. However, the interrelationships span the entire spectrum of cementation options (temporary, semipermanent, and definitive).

Retention of cements is mostly measured with the help of pull-off tests that are performed with a universal testing machine. To increase the clinical relevance of in vitro studies, some studies used clinical removal devices for the pull-off tests [4,45]. However, the measured values are not comparable with the pull-off forces required intraorally. The Coronaflex device is a special tool that uses compressed air to trigger an impact pulse. This acts on the cement and destroys its structure. The retentive strength is dissolved. The superstructure can be removed and usually it is possible to reuse it. A smaller amount of space in the patient's mouth and the fact that Coronaflex is not always straightforward to apply also makes clinical removal of the crowns more difficult, so that more force is required [4]. In vitro, a simplified removal with less force is possible because the device can be freely positioned and rotated. Schierano G, et al., [74] reported that Coronaflex is more repeatable with higher peak amplitudes of forces, which can be considered as positive.

Some studies have performed thermocycling and evaluated the retention forces of the cements tested [9,14,24,40-56]. Thermocycling

has been introduced to imitate artificial ageing. Temperature changes as they occur naturally intraorally can be mimicked easily *in vitro*. The reduction of retention by thermocycling is caused by the regular temperature fluctuations. The thermal stress affects the bonding strength of the cements. Structural changes of the bonds lead to a breakdown of the chemical bond and thus to a failure of the retention between crown and abutment [75]. However, some authors confirmed that thermocycling did not affect retention capacity [53]. Besides, thermocycling is not sufficient for an accurate assessment of the clinical suitability of cements. Long-term mechanical loading (chewing simulation) was only performed to a limited extent [58]. Generally, compressive cyclic loading leads to a reduced retentive strength of cements. Therefore, crowns are easier to remove. Retrievability of the superstructure is achievable, regardless of the cement class [9,54,58,71].

Retentive strength depends on many different factors: the cement type, the cement gap, the cementing technique, the film thickness, the abutment geometry, the surface treatment, and the crown material [3,14,32,42,44,47,49,51,52,55,57,59,61-65,76-91]. In addition, the saliva contamination affects retentive values [48]. Furthermore, many various cements were investigated in different studies with regard to their retention values. Due to noncomparable study protocols and different methodologies, the results cannot reliably be compared.

Conclusion

The present literature review showed that retention of cemented single crowns on implants depends on a lot of different factors. Significant correlations between retentive strength and different parameters (cement type, cleaning and pretreatment of the internal crown surface, taper, abutment surface size, cement gap, grooves on the abutment) could be proven.

Semipermanent cements that have recently appeared on the market have only shown very limited data so far. From today's point of view, it is not yet possible to say whether they have an advantage compared to conventional definitive or provisional cements. Further studies are required to determine the limitations and possibilities of semipermanent cements.

Declarations

Ethics approval and consent to participate: Not applicable.

Consent for publication: Not applicable.

Availability of data and material: All data generated can be found online (see Materials and Methods for the search strategy) at PubMed.

Competing interests: Not applicable.

Funding: Not applicable.

Authors' contributions: Jeremias Hey initiated this review. He supervised the entire preparation of this study, gave groundbreaking ideas and supported the literature research. Martin Rosentritt prepared the statistical analysis concerning the factors influencing the retention force (Table 6) and supported the literature search. Florian Beuer performed the final proofreading of the manuscript and supported the creation of this review with helpful tips regarding structuring and outlining. Elisabeth Prause did the literature research and composed the review.

Acknowledgments: Not applicable.



Table 7: Overview of the included studies with the following information: the cement class used, the material combination between the abutment and the crown, the retention values in Newtons (N), a pretreatment of the crown (alcohol or sandblasting), the particle size of sandblasting in micrometers (μ m), a conducted thermocycling or chewing simulation, the taper in degrees (°), the abutment height in millimeters (mm), the size of the abutment surface in (mm²), the size of the cement gap in mm and the geometry of the abutment in terms of grooves.

Author	Cement	Material (abutment/ crown)	Retention (N)	Pretreatment crown	Particlesize sand- blasting (μm)	Thermo- cycling	Taper (°)	Abutment height (mm)	Chewing simulation	Abutment surface size (mm²)	Cement gap (mm)	Groove (abutment)
	zinc phosphate	titanium- metal alloy	215.73					5.5	yes	33.07		
	zinc phosphate		161.79					5.5	yes	33.07		
	zinc phosphate		311.34	yes	50			5.5	yes	33.07		
	zinc phosphate		253.48	yes	50			5.5	yes	33.07		
	zinc phosphate		383.41	yes				5.5	yes	33.07		
	zinc phosphate		301.53	yes				5.5	yes	33.07		
	zinc phosphate		547.17	yes	50			5.5	yes	33.07		
	zinc phosphate		531.98	yes	50			5.5	yes	33.07		
Al Hamad KQ, et al., [62]	glass ionomer	titanium- metal alloy	183.13			yes	8	4				
	glass ionomer		305.14	yes	50	yes	8	4				
	glass ionomer		239.95			yes	8	6				
	glass ionomer		523.71	yes	50	yes	8	6				
	zinc phosphate		268.59			yes	8	4				
	zinc phosphate		418.69	yes	50	yes	8	4				
	zinc phosphate		647.66			yes	8	6				
	zinc phosphate		700.93	yes	50	yes	8	6				
	zinc oxide eugenol		65.53			yes	8	4				
	zinc oxide eugenol		139.79	yes	50	yes	8	4				
	zinc oxide eugenol		73.48			yes	8	6				
	zinc oxide eugenol		207.09	yes	50	yes	8	6				
	zinc oxide eugenol + petroleum jelly		9.86			yes	8	4				
	zinc oxide eugenol + petroleum jelly		42.09	yes	50	yes	8	4				
	zinc oxide eugenol + petroleum jelly		17.36			yes	8	6				
	zinc oxide eugenol + petroleum jelly		48.27	yes	50	yes	8	6				
Abbo B, et al., [63]	resin based	titanium- zirconia	124.89					5.5		33.07		
	resin based		198.09					6.5		36.03		
Carnaggio TV, et al [59]	zinc oxide noneugenol	titanium- zirconia	83							42	100	
	zinc oxide noneugenol		82							60	100	
	zinc oxide noneugenol		114							82	100	
	resin based		92							42	100	
	resin based		127							60	100	
	resin based		104							82	100	
	glass ionomer		96							42	100	
	glass ionomer		84							60	100	



	glass ionomer		56						82	100	
	resin based		199						42	100	
	resin based		241						60	100	
	resin based		246						82	100	
	resin based		184						 42	100	
	resin based		237						 60	100	
	resin based		318						 82	100	
Derafshi R, et al., [65]	zinc oxide eugenol	titanium- metal alloy	46.88					5.5	 31.64	20	
	zinc oxide eugenol		46.31					5.5	 31.64	20	
	zinc oxide eugenol		65.3					5.5	31.64	20	
	zinc oxide eugenol		62.25					5.5	31.64	20	
Gultekin P, et al., [13]	resin based	titanium- metal alloy	136.97	yes	50			6.5	30.77	20	
	resin based		139.5	yes	50			6.5	 30.77	20	
	resin based		155.79	yes	50			6.5	 30.77	20	
	resin based		150.28	yes	50			6.5	 30.77	20	
	resin based		86.16	yes	50			6.5	 30.77	20	
	resin based		105.66	yes	50			6.5	 30.77	20	
	resin based		301.6	yes	50			6.5	 30.77	20	
	zinc oxide noneugenol		39.65	yes	50			6.5	 30.77	20	
	resin based		171.35	yes	50			6.5	30.77	40	
	resin based		179.54	yes	50			6.5	30.77	40	
	resin based		187.3	yes	50			6.5	30.77	40	
	resin based		190.75	yes	50			6.5	 30.77	40	
	resin based		83.63	yes	50			6.5	 30.77	40	
	resin based		118.57	yes	50			6.5	 30.77	40	
	resin based		378.85	yes	50			6.5	 30.77	40	
	zinc oxide noneugenol		42.72	yes	50			6.5	30.77	40	
Gumus HO, et al., [41]	zinc oxide eugenol	titanium- metal alloy	45.1	yes			6	2	17.97		
	zinc oxide noneugenol		90.7	yes			6	2	 17.97		
	resin based		36.1	yes			6	2	17.97		
	zinc oxide eugenol		34.4	yes			6	2	 17.97		
	glass ionomer		82.8	yes			6	2	 17.97		
	zinc oxide noneugenol		67.7	yes			6	2	 17.97		
	zinc oxide eugenol		23.3	yes		yes	6	2	17.97		
	zinc oxide noneugenol		6.2	yes		yes	6	2	17.97		
	resin based		8.8	yes		yes	6	2	17.97		
	zinc oxide eugenol		12.7	yes		yes	6	2	 17.97		
	glass ionomer		32.9	yes		yes	6	2	17.97		
	zinc oxide noneugenol		24.6	yes		yes	6	2	17.97		
Güncü MB, et al., [24]	zinc oxide noneugenol	titanium- metal alloy	33.7	yes	50	yes			48.29	25.4	
	zinc phosphate		262.6	yes	50	yes			48.29	25.4	



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	glass ionomer		75.7	yes	50	yes			48.29	25.4	
	zinc oxide noneugenol		20.5	yes	50	yes			90	25.4	
	zinc phosphate		258	yes	50	yes			90	25.4	
	glass ionomer		42.1	yes	50	yes			90	25.4	
Jugdev J, et al., [85]	zinc oxide eugenol	titanium- metal alloy	120	yes	50						
	zinc oxide eugenol		140	yes	50						
	resin based		150	yes	50						
	resin based		300	yes	50						
	resin based		150	yes	50						
	resin based		360	yes	50						
Kilicarslan MA, et al., [83]	resin based	titanium- metal alloy	455.1		50		6	5.7	37.53	20	
	resin based		565.52		50		6	5.7	37.53	20	
	resin based		534.78		50		6	5.7	37.53	20	
	resin based		678.6		50		6	5.7	37.53	20	
Kim Y, et al., [32]	calcium-hydroxide	titanium- PMMA	48					4			
	calcium-hydroxide		58					4			
	calcium-hydroxide		52					4			
	zinc oxide noneugenol		39					4			
	zinc oxide noneugenol		53					4			
	zinc oxide noneugenol		40					4			
	zinc oxide eugenol		11					4			
	zinc oxide eugenol		20					4			
	zinc oxide eugenol		23					4			
	zinc oxide eugenol		10					4			
	zinc oxide eugenol		12					4			
	zinc oxide eugenol		14					4			
Kokubo Y, et al., [14]	polycarboxylate	zirconia- zirconia	300	yes			8	7.4	51.39		
	polycarboxylate		120	yes		yes	8	7.4	51.39		
	polycarboxylate		250	yes	50		8	7.4	51.39		
	polycarboxylate		275	yes	50	yes	8	7.4	51.39		
	polycarboxylate		60	yes			8	7.4	51.39		
	polycarboxylate		40	yes		yes	8	7.4	51.39		
	polycarboxylate		50	yes	50		8	7.4	51.39		
	polycarboxylate		20	yes	50	yes	8	7.4	51.39		
	zinc oxide eugenol		100	yes			8	7.4	51.39		
	zinc oxide eugenol		60	yes		yes	8	7.4	51.39		
	zinc oxide eugenol		70	yes	50		8	7.4	51.39		
	zinc oxide eugenol		70	yes	50	yes	8	7.4	51.39		
	zinc oxide noneugenol		120	yes			8	7.4	51.39		
	zinc oxide noneugenol		10	yes		yes	8	7.4	51.39		



	zinc oxide noneugenol		80	yes	50		8	7.4	51.39		
	zinc oxide noneugenol		5	yes	50	yes	8	7.4	51.39		
	zinc oxide eugenol		60	yes			8	7.4	51.39		
	zinc oxide eugenol		10	yes		yes	8	7.4	51.39		
	zinc oxide eugenol		70	yes	50		8	7.4	51.39		
	zinc oxide eugenol		40	yes	50	yes	8	7.4	51.39		
Kurt M, et al., [42]	resin based	titanium- metal alloy	249.41			yes		4			
	resin based		315.14			yes		4	 		
	resin based		506.02	yes	50	yes		4			
	resin based		223.26			yes		4			
	resin based		412.91			yes		4			
Lennartz A, et al., [43]	zinc oxide eugenol	zirconia- zirconia	234	yes	50		6	6	 34.55		
	resin based		110	yes	50		6	6	 34.55		
	resin based		103	yes	50		6	6	34.55		
	resin based		61	yes	50		6	6	34.55		
	resin based		49	yes	50		6	6	 34.55		
	zinc oxide eugenol		20	yes	50	yes	6	6	34.55		
	resin based		10	yes	50	yes	6	6	34.55		
	resin based		10	yes	50	yes	6	6	 34.55		
	resin based		25	yes	50	yes	6	6	 34.55		
	resin based		10	yes	50	yes	6	6	 34.55		
Lewinstein I, et al., [44]	zinc oxide noneugenol	titanium- metal alloy	170	yes	110	yes	6	6			
	zinc phosphate		362	yes	110	yes	6	6			
	zinc oxide noneugenol		188	yes	110	yes	6	6			yes
	zinc phosphate		580	yes	110	yes	6	6			yes
	zinc oxide noneugenol		204	yes	110	yes	6	6			yes
	zinc phosphate		549	yes	110	yes	6	6			yes
	zinc oxide noneugenol		242	yes	110	yes	6	6			yes
	zinc phosphate		587	yes	110	yes	6	6			yes
Mehl C, et al., [45]	glass ionomer	titanium- metal alloy	292	yes	50		5	6	 34.55		yes
	glass ionomer		264	yes	50	yes	5	6	34.55		yes
	polycarboxylate		556	yes	50		5	6	 34.55		yes
	polycarboxylate		471	yes	50	yes	5	6	 34.55		yes
Mehl C, et al., [3]	glass ionomer	titanium- metal alloy	605	yes	50		6	4	28.78	20	
	glass ionomer		144	yes	50		6	4	28.78	50	
	glass ionomer		104	yes	50		6	4	28.78	80	
	glass ionomer		105	yes	50		6	4	28.78	110	
	polycarboxylate		1041	yes	50		6	4	 28.78	20	
	polycarboxylate		307	yes	50		6	4	28.78	50	
	polycarboxylate		94	yes	50		6	4	28.78	80	



	polycarboxylate		96	yes	50		6	4		28.78	110	
	resin based		1237	yes	50		6	4		28.78	20	
	resin based		480	yes	50		6	4		28.78	50	
	resin based		448	yes	50		6	4		28.78	80	
	resin based		362	yes	50		6	4		28.78	110	
Mehl C, et al., [46]	glass ionomer	titanium- metal alloy	244	yes	50		6	4		28.78		
	resin based		307	yes	50		6	4		28.78		
	resin based		154	yes	50		6	4		28.78		
	resin based		107	yes	50		6	4		28.78		
	glass ionomer		264	yes	50	yes	6	4		28.78		
	resin based		311	yes	50	yes	6	4		28.78		
	resin based		93	yes	50	yes	6	4		28.78		
	resin based		81	yes	50	yes	6	4		28.78		
	glass ionomer		225	yes	50		6	4	yes	28.78		
	resin based		275	yes	50		6	4	yes	28.78		
	resin based		123	yes	50		6	4	yes	28.78		
	resin based		81	yes	50		6	4	yes	28.78		
	glass ionomer		235	yes	50	yes	6	4	yes	28.78		
	resin based		303	yes	50	yes	6	4	yes	28.78		
	resin based		102	yes	50	yes	6	4	yes	28.78		
	resin based		86	yes	50	yes	6	4	yes	28.78		
Nagasawa Y, et al., [67]	polycarboxylate	titanium-gold	72	yes	50		10	5		37.2	50	
	polycarboxylate		76	yes	50		10	5		37.2	50	
	polycarboxylate		110	yes	50		10	5		37.2	50	
	polycarboxylate		72	yes	50		10	5		37.2	50	
	zinc oxide eugenol		93	yes	50		10	5		37.2	50	
	zinc oxide eugenol		81	yes	50		10	5		37.2	50	
	zinc oxide noneugenol		82	yes	50		10	5		37.2	50	
	zinc oxide noneugenol		70	yes	50		10	5		37.2	50	
	zinc oxide eugenol		48	yes	50		10	5		37.2	50	
	zinc oxide eugenol		25	yes	50		10	5		37.2	50	
	zinc oxide eugenol		26	yes	50		10	5		37.2	50	
	zinc oxide eugenol		20	yes	50		10	5		37.2	50	
Naumova EA, et al. [47]	zinc oxide noneugenol	titanium- metal alloy	191.7	yes	50		6	5.8		33.95		
	glass ionomer		902.3	yes	50		6	5.8		33.95		
	glass ionomer		863.6	yes	50		6	5.8		33.95		
	zinc phosphate		615.8	yes	50		6	5.8		33.95		
	glass ionomer		740.1	yes	50		6	5.8		33.95		
	glass ionomer		588.5	yes	50		6	5.8		33.95		
	resin based		334.5	yes	50		6	5.8		33.95		
	glass ionomer		642.2	yes	50		6	5.8		33.95		
	zinc oxide noneugenol		49.09	yes	50		6	5.8		33.95		

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	glass ionomer		213.6	yes	50		6	5.8		33.95		
	glass ionomer		251.4	yes	50		6	5.8		33.95		
	zinc phosphate		258.1	yes	50		6	5.8		33.95		
	glass ionomer		242.4	yes	50		6	5.8		33.95		
	glass ionomer		249.2	yes	50		6	5.8		33.95		
	resin based		205	yes	50		6	5.8		33.95		
	glass ionomer		229.1	yes	50		6	5.8		33.95		
	zinc oxide noneugenol		30.98	yes	50		6	5.8		33.95		
	glass ionomer		179.3	yes	50		6	5.8		33.95		
	glass ionomer		165.3	yes	50		6	5.8		33.95		
	zinc phosphate		185.3	yes	50		6	5.8		33.95		
	glass ionomer		178.8	yes	50		6	5.8		33.95		
	glass ionomer		188.6	yes	50		6	5.8		33.95		
	resin based		158.9	yes	50		6	5.8		33.95		
	glass ionomer		150.6	yes	50		6	5.8		33.95		
Nejatidanse F, et al., [49]	resin based	titanium- zirconia	203.49	yes	110	yes	8	5.5				
	resin based		190.61	yes	110	yes	8	5.5				
	resin based		172.16	yes	110	yes	8	5.5				
	zinc phosphate		72.01	yes	110	yes	8	5.5				
	polycarboxylate		44.18	yes	110	yes	8	5.5				
	glass ionomer		3.12	yes	110	yes	8	5.5				
	zinc oxide		11.27	yes	110	yes	8	5.5				
	zinc oxide eugenol		4.52	ves	110	ves	8	5.5				
	resin based		4.03	ves	110	ves	8	5.5				
Nejatidanse F, et al., [48]	resin based	titanium- zirconia	183.9	yes		yes	6	5.5			30	
	resin based		123.64	yes		yes	6	5.5			30	
	resin based		190.57	yes		yes	6	5.5			30	
	resin based		195.43	yes	50	yes	6	5.5			30	
	resin based		204.79	yes		yes	6	5.5			30	
	resin based		232.65	yes		yes	6	5.5			30	
	resin based		193.11	yes		yes	6	5.5			30	
Ongthiemsak, et al., [57]	zinc oxide eugenol	titanium-gold	39.94	yes	50				yes			
	zinc oxide eugenol		43.77	yes	50				yes			
	zinc oxide eugenol		47.47	yes	50				yes			
Pan YH, et al., [16]	resin based + petroleum jelly	titanium- metal alloy	32	yes	50	yes		12	yes			
	zinc oxide eugenol		36.6	yes	50	yes		12	yes			
	resin based		39.2	yes	50	yes		12	yes			
	zinc oxide noneugenol		40.8	yes	50	yes		12	yes			
	resin based		45.4	yes	50	yes		12	yes			
	zinc phosphate + petroleum jelly		147	yes	50	yes		12	yes			
	zinc phosphate		249.2	yes	50	yes		12	yes			

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Pitta J, et al., [52]	resin based	titanium- PMMA	64.1	yes		yes					
	resin based		64.9	yes	50	yes					
	resin based		276.7	yes	30	yes					
	resin based		39.1	yes	30	yes					
	resin based		1146.5	yes		yes					
Pitta J, et al., [53]	resin based	titanium- PMMA	206.3			yes		yes			
	resin based		346.9			yes		yes			
	resin based		420			yes		yes			
	resin based		376.1			yes		yes			
Reddy SV, et al., [68]	zinc oxide eugenol	titanium- metal alloy	258.28	yes	50						
	zinc oxide eugenol		260.68	yes	50						
	zinc oxide eugenol		138.41	yes	50						
	zinc oxide eugenol		138.28	yes	50						
	resin based		184.86	yes	50						
	resin based		152.13	yes	50						
Rödiger M, et al., [25]	resin based	titanium- zirconia	101.1	yes	110	yes	4.31				
	resin based		311.7	yes	110	yes	6.79				
	resin based		447.9	yes	110	yes	4.31				
	resin based		478.7	yes	110	yes	6.79				
Rohr N, et al., [72]	glass ionomer	zirconia- zirconia	196	yes							
	resin based		43	yes							
	zinc oxide eugenol		127	yes							
	resin based		261	yes							
	resin based		253	yes							
	resin based		270	yes							
	resin based		226	yes							
	resin based		222	yes							
	resin based		238	yes							
	resin based		245	yes							
	resin based		318	yes							
	resin based		254	yes							
	resin based		605	yes							
	resin based		470	yes							
	resin based		257	yes							
	resin based		243	yes							
	resin based		269	yes							
	resin based		224	yes							
	resin based		363	yes							
	resin based		288	yes							
Rues S, et al [54]	zinc oxide	zirconia- zirconia	31	yes	50		4				
, [• .]	methacrylate based		40	yes	50		4				
	resin based		436	ves	50		4				
	zinc phosphate		682	ves	50		 4				
				,		1				1	



	glass ionomer		425	yes	50			4			
	zinc oxide noneugenol		17	yes	50	yes		4			
	methacrylate based		8	yes	50	yes		4			
	resin based		590	yes	50	yes		4			
	zinc phosphate		656	yes	50	yes		4			
	glass ionomer		522	yes	50	yes		4			
	zinc oxide noneugenol		107	yes	50			5.5			
	methacrylate based		41	yes	50			5.5			
	resin based		596	yes	50			5.5			
	zinc phosphate		477	yes	50			5.5			
	glass ionomer		570	yes	50			5.5			
	zinc oxide noneugenol		11	yes	50	yes		5.5			
	methacrylate based		13	yes	50	yes		5.5			
	resin based		689	yes	50	yes		5.5			
	zinc phosphate		915	yes	50	yes		5.5			
	glass ionomer		757	yes	50	yes		5.5			
Sadig wM, et al., [89]	zinc phosphate	titanium- titanium	380	yes	50			5.5			
	zinc phosphate		180	yes	50			5.5			
	zinc phosphate		260	yes	50			5.5			
	resin based		310	yes	50			5.5			
	resin based		470	yes	50			5.5			
	resin based		500	yes	50			5.5			
Safari S, et al., [61]	resin based	titanium- metal alloy	364.19	yes		yes		3	27.69	30	
	glass ionomer		154.02	yes		yes		3	27.69	30	
	zinc oxide eugenol		115.99	yes		yes		3	27.69	30	
	resin based		352.84	yes		yes		3	27.69	30	
	resin based		460.44	yes		yes		3	31.9	30	
	glass ionomer		243.68	yes		yes		3	 31.9	30	
	zinc oxide eugenol		164.7	yes		yes		3	31.9	30	
	resin based		405.45	yes		yes		3	31.9	30	
Sahu N, et al., [82]	resin based	titanium- metal alloy	408.3	yes	110			8		25	
	resin based		159.9	yes	110			8		25	
	resin based		743.8	yes	110			8		25	
Schiessl C, et al., [55]	polycarboxylate	titanium- metal alloy	400	yes	50		4	6	33.12		
	polycarboxylate		430	yes	50		4	6	33.12		
	polycarboxylate		200	yes	50		4	6	33.12		
	zinc phosphate		270	yes	50		4	6	33.12		
	methacrylate based		80	yes	50		4	6	33.12		
	glass ionomer		180	yes	50		4	6	33.12		
	resin based		270	yes	50		4	6	33.12		
	zinc oxide noneugenol		130	yes	50		4	6	33.12		
	polycarboxylate		380	yes	50		6	6	33.12		



polycarboxylate	240	yes	50		6	6	33.12	
polycarboxylate	200	yes	50		6	6	33.12	
zinc phosphate	200	yes	50		6	6	33.12	
methacrylate based	110	yes	50		6	6	33.12	
glass ionomer	120	yes	50		6	6	33.12	
resin based	230	yes	50		6	6	33.12	
zinc oxide noneugenol	100	yes	50		6	6	33.12	
polycarboxylate	320	yes	50		8	6	33.12	
polycarboxylate	140	yes	50		8	6	33.12	
polycarboxylate	140	yes	50		8	6	33.12	
zinc phosphate	160	yes	50		8	6	33.12	
polycarboxylate	80	yes	50		8	6	33.12	
glass ionomer	100	yes	50		8	6	33.12	
resin based	260	yes	50		8	6	33.12	
zinc oxide noneugenol	90	yes	50		8	6	33.12	
polycarboxylate	660	yes	50	yes	4	6	33.12	
polycarboxylate	380	yes	50	yes	4	6	33.12	
polycarboxylate	400	yes	50	yes	4	6	33.12	
zinc phosphate	370	yes	50	yes	4	6	33.12	
methacrylate based	5	yes	50	yes	4	6	33.12	
glass ionomer	300	yes	50	yes	4	6	33.12	
resin based	300	yes	50	yes	4	6	33.12	
zinc oxide noneugenol	50	yes	50	yes	4	6	33.12	
polycarboxylate	580	yes	50	yes	6	6	33.12	
polycarboxylate	400	yes	50	yes	6	6	33.12	
polycarboxylate	210	yes	50	yes	6	6	33.12	
zinc phosphate	280	yes	50	yes	6	6	33.12	
methacrylate based	5	yes	50	yes	6	6	33.12	
glass ionomer	250	yes	50	yes	6	6	33.12	
resin based	240	yes	50	yes	6	6	33.12	
zinc oxide noneugenol	40	yes	50	yes	6	6	33.12	
polycarboxylate	620	yes	50	yes	8	6	33.12	
polycarboxylate	400	yes	50	yes	8	6	33.12	
polycarboxylate	250	yes	50	yes	8	6	33.12	
zinc phosphate	250	yes	50	yes	8	6	33.12	
methacrylate based	5	yes	50	yes	8	6	33.12	
glass ionomer	200	yes	50	yes	8	6	33.12	
resin based	210	yes	50	yes	8	6	33.12	
zinc oxide noneugenol	50	yes	50	yes	8	6	33.12	
zinc phosphate	300	yes	50		4	6	33.12	
glass ionomer	110	yes	50		4	6	33.12	
zinc oxide noneugenol	100	yes	50		4	6	33.12	



resin based	250	yes	50		4	6	33.1	2	
zinc phosphate	210	yes	50		6	6	33.1	2	
glass ionomer	100	yes	50		6	6	33.1	2	
zinc oxide noneugenol	110	yes	50		6	6	33.1	2	
resin based	270	yes	50		6	6	33.1	2	
zinc phosphate	180	yes	50		8	6	33.1	2	
glass ionomer	90	yes	50		8	6	33.1	2	
zinc oxide noneugenol	80	yes	50		8	6	33.1	2	
 resin based	260	yes	50		8	6	33.1	2	
zinc phosphate	280	yes	50	yes	4	6	33.1	2	
 glass ionomer	300	yes	50	yes	4	6	33.1	2	
zinc oxide noneugenol	70	yes	50	yes	4	6	33.1	2	
resin based	320	yes	50	yes	4	6	33.1	2	
zinc phosphate	230	yes	50	yes	6	6	33.1	2	
glass ionomer	180	yes	50	yes	6	6	33.1	2	
zinc oxide noneugenol	50	yes	50	yes	6	6	33.1	2	
resin based	290	yes	50	yes	6	6	33.1	2	
 zinc phosphate	250	yes	50	yes	8	6	33.1	2	
glass ionomer	190	yes	50	yes	8	6	33.1	2	
zinc oxide	40	yes	50	yes	8	6	33.1	2	
 noneugenoi	280	Ves	50	Ves	8	6	33.1	2	
	380	yes	120	yes		6	33.1	2	
glass ionomer	210	yes	120		4	6	33.1	2	
 zinc oxide	90	ves	120		4	6	33.1	2	
 noneugenol	200	,	120			6	22.1	2	
 resin based	260	yes	120		4	6	33.1	2	
zinc phosphate	350	yes	120		6	6	33.1	2	
 glass lonomer	190	yes	120		6	6	33.1	.2	
noneugenol	110	yes	120		6	6	33.1	.2	
resin based	210	yes	120		6	6	33.1	2	
zinc phosphate	340	yes	120		8	6	33.1	.2	
glass ionomer	160	yes	120		8	6	33.1	2	
zinc oxide noneugenol	100	yes	120		8	6	33.1	2	
resin based	220	yes	120		8	6	33.1	.2	
zinc phosphate	350	yes	120		4	6	33.1	.2	
glass ionomer	220	yes	120		4	6	33.1	2	
zinc oxide noneugenol	40	yes	120		4	6	33.1	2	
resin based	260	yes	120		4	6	33.1	2	
zinc phosphate	280	yes	120		6	6	33.1	2	
glass ionomer	220	yes	120		6	6	33.1	2	
zinc oxide noneugenol	40	yes	120		6	6	33.1	2	
resin based	210	yes	120		6	6	33.1	2	
zinc phosphate	280	yes	120		8	6	33.1	2	



glass ionomer	210	yes	120		8	6	33.12	
zinc oxide noneugenol	20	yes	120		8	6	33.12	
resin based	220	yes	120		8	6	33.12	
polycarboxylate	150	yes	50		4	6	33.12	
polycarboxylate	220	yes	50		4	6	33.12	
polycarboxylate	225	yes	50		4	6	33.12	
polycarboxylate	100	yes	50		6	6	33.12	
polycarboxylate	75	yes	50		6	6	33.12	
polycarboxylate	160	yes	50		6	6	33.12	
polycarboxylate	110	yes	50		8	6	33.12	
polycarboxylate	80	yes	50		8	6	33.12	
polycarboxylate	160	yes	50		8	6	33.12	
polycarboxylate	140	yes	50	yes	4	6	33.12	
polycarboxylate	290	yes	50	yes	4	6	33.12	
polycarboxylate	330	yes	50	yes	4	6	33.12	
polycarboxylate	225	yes	50	yes	6	6	33.12	
polycarboxylate	240	yes	50	yes	6	6	33.12	
polycarboxylate	225	yes	50	yes	6	6	33.12	
polycarboxylate	60	yes	50	yes	8	6	33.12	
polycarboxylate	350	yes	50	yes	8	6	33.12	
polycarboxylate	225	yes	50	yes	8	6	33.12	
polycarboxylate	380	yes	50		4	6	33.12	
polycarboxylate	400	yes	50		4	6	33.12	
polycarboxylate	220	yes	50		4	6	33.12	
polycarboxylate	375	yes	50		6	6	33.12	
polycarboxylate	230	yes	50		6	6	33.12	
polycarboxylate	210	yes	50		6	6	33.12	
polycarboxylate	300	yes	50		8	6	33.12	
polycarboxylate	90	yes	50		8	6	33.12	
polycarboxylate	100	yes	50		8	6	33.12	
polycarboxylate	610	yes	50	yes	4	6	33.12	
polycarboxylate	375	yes	50	yes	4	6	33.12	
polycarboxylate	390	yes	50	yes	4	6	33.12	
polycarboxylate	520	yes	50	yes	6	6	33.12	
polycarboxylate	380	yes	50	yes	6	6	33.12	
polycarboxylate	220	yes	50	yes	6	6	33.12	
polycarboxylate	610	yes	50	yes	8	6	33.12	
polycarboxylate	390	yes	50	yes	8	6	33.12	
polycarboxylate	220	yes	50	yes	8	6	33.12	
polycarboxylate	470	yes	50		4	6	33.12	
polycarboxylate	375	yes	50		4	6	33.12	
polycarboxylate	220	yes	50		4	6	33.12	
polycarboxylate	520	yes	50		6	6	33.12	



	polycarboxylate		330	yes	50		6	6	33.12	
	polycarboxylate		280	yes	50		6	6	33.12	
	polycarboxylate		400	yes	50		8	6	33.12	
	polycarboxylate		300	yes	50		8	6	33.12	
	polycarboxylate		225	yes	50		8	6	33.12	
	polycarboxylate		610	yes	50	yes	4	6	33.12	
	polycarboxylate		350	yes	50	yes	4	6	33.12	
	polycarboxylate		330	yes	50	yes	4	6	33.12	
	polycarboxylate		520	yes	50	yes	6	6	33.12	
	polycarboxylate		230	yes	50	yes	6	6	33.12	
	polycarboxylate		250	yes	50	yes	6	6	33.12	
	polycarboxylate		580	yes	50	yes	8	6	33.12	
	polycarboxylate		360	yes	50	yes	8	6	33.12	
	polycarboxylate		220	yes	50	yes	8	6	33.12	
Sheets JL, et al., [66]	zinc oxide eugenol	titanium- metal alloy	117.8	yes	50		3	6.38		
	polycarboxylate		358.6	yes	50		3	6.38		
	resin based + petroleum jelly		130.8	yes	50		3	6.38		
	resin based		172.4	yes	50		3	6.38		
	resin based + KY jelly		31.6	yes	50		3	6.38		
	resin based		131.6	yes	50		3	6.38		
	resin based		41.2	yes	50		3	6.38		
	zinc phosphate		171.8	yes	50		3	6.38		
	glass ionomer		167.8	yes	50		3	6.38		
	glass ionomer		147.5	yes	50		3	6.38		
	polycarboxylate		158.8	yes	50		3	6.38		
Guler U, et al., [9]	zinc oxide eugenol	titanium- zirconia	6.52			yes				
	zinc phosphate		83.09			yes				
	resin based		251.18			yes				
	zinc oxide eugenol		17.82			yes				
	zinc phosphate		116.41			yes				
	resin based		248.72			yes				

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